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F. Esmailie, M. Francoeur, T. A. Ameel

Department of Mechanical Engineering, University of Utah, Salt Lake City, UT, USA

Corresponding author: <u>ameel@mech.utah.edu</u>, Presenting author: <u>fateme.esmailie@utah.edu</u>



0.8

×10⁻³





Magnetically-guided, robotic assisted insertion [2] Reduces risk of intracochlear physical trauma Risk: thermal trauma in the magnet detachment phase

Goals:

- Use Comsol Multiphysics 5.3a to study heat transfer within the cochlea to determine safe conditions for magnet removal.
- Verify Comsol Multiphysics 5.3a solutions for intracochlear temperature with analytical solutions.



Figure 3. 1-D model validation of the 2-D numerical model in the mid-cochlea cross-section, z = 17.5 mm.

r (m)

0.4

0.6

0.2



Figure 1. Simplification of a 3-D cochlea in (a) 1-D and (b) 2-D models [3].





Figure 4. (a) Maximum operation time (t_{max}) as a function of power input (g_0) for a safe temperature of 316 K. (b) Maximum temperature (T_{max}) as a function of power input (g_0) for an exposure time of 114 s.

CONCLUSIONS

The maximum temperature difference between the analytical and

Analytical solution	Numerical solution
Solution method: Green's function Programming language: MATLAB R2018a	Software: COMSOL Multiphysics 5.3a Physics: Heat transfer in solids Study: Time dependent

RESULTS

Thermal damage threshold of in-vivo tissues depends on:

type of tissue

temperature (T)

heat source exposure time (t)

For ear tissues: **T**= 316 K and **t** = 114 s [4].

numerical solutions is less than 2% (Figs. 2 and 3).

Maximum safe allowable power input for magnet detachment from cochlear implant is 1.35 × 10⁷ W/m³ (Fig. 4).
These results (and others) will eventually help assess the accuracy of a

complex 3-D transient heat transfer model of the cochlea.

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